

Please delete claim 1-27, and add new claims 28-106 as follows:

28. An ultrasound imaging system for producing a 3 dimensional image of ^{two or three} ultrasound reflectors inside a body, comprising:

- an ultrasound transducer;
- an ultrasound transmitter coupled to the ultrasound transducer, the ultrasound transducer being operable to generate a signal having a fundamental frequency;
- an ultrasound receiver coupled to the ultrasound transducer, the ultrasound receiver being operable to receive a signal from the ultrasound transducer corresponding to ultrasound reflections from ^{the use of three} ultrasound reflectors at a plurality of depths in the body;
- a filter coupled to the ultrasound receiver, the filter being operable to selectively pass signals received by the receiver having a frequency that is a harmonic of the fundamental frequency and to provide an output signal corresponding thereto; and
- an image processor coupled to receive the output signal from the filter, the image processor being operable to generate a ^{three -} 3 dimensional image from the output signal of the filter.

29. The ultrasonic imaging system of claim 28 wherein the filter is further operable to pass signals at the fundamental frequency so that the output signal is a combination of signals received by the receiver having the fundamental frequency and signals received by the receiver having the harmonic frequency.

30. The ultrasonic imaging system of claim 29 wherein the filter further comprises:

a low frequency channel operable to pass components of the signals received by the receiver having the fundamental frequency;

a high frequency channel operable to pass components of the signals received by the receiver having the harmonic frequency; and

a combiner operable to combine the signals passed through the low frequency channel and the signals passed through the high frequency channel.

31. The ultrasonic imaging system of claim 30 wherein the low frequency channel is further operable to attenuate signals reflected from ultrasound reflectors at

shallower depths of the body to a greater extent than signals reflected from ultrasound reflectors at greater depths of the body, and the high frequency channel is further operable to attenuate signals reflected from ultrasound reflectors at greater depths of the body to a greater extent than signals reflected from ultrasound reflectors at shallower depths of the body so that deeper portions of the 3-dimensional image are produced predominantly from signals received by the receiver having the fundamental frequency and shallower portions of the 3-dimensional image are produced predominantly from signals received by the receiver having the harmonic frequency.

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32. The ultrasonic imaging system of claim 31 wherein the high frequency channel includes a depth-dependent time varying filter to attenuate signals passing through the channel as a function of depth of the body.

33. The ultrasonic imaging system of claim 28 wherein the ultrasound reflectors comprise tissue or fluid, and wherein the three dimensional image is generated in the absence of an ultrasound contrast agent.

34. The ultrasound imaging system of claim 30 wherein the combiner comprises a switch operable to alternatively couple either the low frequency channel or the high frequency channel to the image processor.

35. The ultrasound imaging system of claim 30 wherein the combiner comprises a summing device operable to generate a composite signal formed from both a fundamental frequency signal coupled through the low frequency channel and a harmonic frequency signal coupled through the high frequency channel.

36. The ultrasound imaging system of claim 28 further comprising a Doppler processor coupling the image processor to the filter, the Doppler processor being operable to generate a Doppler signal from the output signal of the filter, the Doppler signal being applied to the image processor so that the 3 dimensional image corresponds to ultrasound reflections from moving ultrasound reflectors.

37. The ultrasound imaging system of claim 36 wherein the Doppler signal is indicative of the velocity of the moving ultrasound reflectors.

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40. The ultrasound imaging system of claim 28 wherein the filter
nite impulse response filter operable to filter and decimate the signals received

41. The ultrasound imaging system of claim 28 wherein the transmitter is operable to generate first and second successive pulses of signals at the fundamental frequency having different phases, and wherein the filter comprises a signal processor operable to combine a first signal received from the receiver resulting from the first successive pulse with a second signal received from the receiver resulting from the second successive pulse.

42. The ultrasound imaging system of claim 28 wherein the signal generated by the ultrasound transmitter has a range of frequency components, the range of frequency components including the fundamental frequency.

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an ultrasonic transducer operable to transmit ultrasonic pulses into a body and receive echo signals responsive to the pulses, the ultrasonic pulses having a fundamental frequency component;

a beamformer coupled to receive the echo signals from the ultrasonic transducer and to generate output signals corresponding thereto;

a filter coupled to receive the output signals from the beamformer, the filter being operable to selectively pass harmonic frequency components of the beamformer output signals that are a harmonic of the fundamental frequency component; and

an image processor coupled to the filter to receive the harmonic frequency components of the beamformer output signals, the image processor being operable to generate a 3 dimensional image from the harmonic frequency components of the beamformer output signals.

44. The ultrasonic imaging system of claim 43 wherein the filter comprises a digital filter.

45. The ultrasonic imaging system of claim 43 wherein the filter is further operable to pass fundamental frequency components of the beamformer output signals so that the image is formed from fundamental and harmonic frequency components of the beamformer output signals.

46. The ultrasonic imaging system of claim 45 wherein the filter comprises:

a low frequency channel operable to pass the fundamental frequency components;

a high frequency channel operable to pass the harmonic frequency components; and

a combiner operable to combine the fundamental frequency components with the harmonic frequency components.

47. The ultrasonic imaging system of claim 46 wherein the low frequency channel is further operable to attenuate signals reflected from ultrasound reflectors at shallower depths of the body to a greater extent than signals reflected from ultrasound reflectors at greater depths of the body, and the high frequency channel is further operable to attenuate signals reflected from ultrasound reflectors at greater depths of the body to a greater extent than signals reflected from ultrasound reflectors at shallower depths of the body so that deeper portions of the 3-dimensional image are produced predominantly from the fundamental frequency components and shallower portions of the 3-dimensional image are produced predominantly from the harmonic frequency components.

48. The ultrasonic imaging system of claim 46 wherein the high frequency channel each includes a depth-dependent time varying filter to attenuate signals passing through the channel as a function of the depth from which the echo signals are received.

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49. The ultrasonic imaging system of claim 46 wherein the low frequency channel is operable to attenuate signals reflected from ultrasound reflectors at a first range of depths to a greater extent than signals reflected from ultrasound reflectors at a second range of depths, and to attenuate signals reflected from ultrasound reflectors at the second range of depths to a greater extent than signals reflected from ultrasound reflectors at a third range of depths, and wherein the high frequency channel is operable to attenuate signals reflected from ultrasound reflectors at the third range of depths to a greater extent than signals reflected from ultrasound reflectors at the second range of depths, and to attenuate signals reflected from ultrasound reflectors at the second range of depths to a greater extent than signals reflected from ultrasound reflectors at the first range of depths, the third range of depths being deeper than the second range of depths, and the second range of depths being deeper than the first range of depths so that portions of the 3-dimensional image in the third range of depths are produced predominantly from the fundamental frequency component, portions of the 3-dimensional image in the first range of depths of the body are produced predominantly from the harmonic frequency component, and portions of the 3-dimensional image in the second range of depths are produced substantially equally from the fundamental frequency component and the harmonic frequency component.

50. The ultrasonic imaging system of claim 46 wherein the combiner comprises a switch operable to alternatively couple either the low frequency channel or the high frequency channel to the image processor.

51. The ultrasonic imaging system of claim 46 wherein the combiner comprises a summing device operable to generate a composite signal formed from both the fundamental frequency component coupled through the low frequency channel and the harmonic frequency component coupled through the high frequency channel.

52. The ultrasonic imaging system of claim 43 further comprising a Doppler processor coupling the image processor to the filter, the Doppler processor being operable to generate a Doppler signal from the harmonic frequency component, the Doppler

53. The ultrasonic imaging system of claim 52 wherein the Doppler signal is indicative of the velocity of the moving ultrasonic reflectors.

54. The ultrasonic imaging system of claim 52 wherein the Doppler signal is indicative of the intensity of reflections from the moving ultrasonic reflectors

55. The ultrasonic imaging system of claim 43 wherein the filter is further operable to shift the frequency of the harmonic frequency component.

56. The ultrasonic imaging system of claim 43 wherein the filter comprises a finite impulse response filter operable to filter and decimate the beamformer output signals.

57. The ultrasonic imaging system of claim 43 wherein the ultrasonic pulses comprise first and second successive pulses of signals having the fundamental frequency component, the first and second pulses having different phases, and wherein the filter comprises a signal processor operable to combine a first output signal from the beamformer derived from an echo signal responsive to the first successive pulse with a second signal from the beamformer derived from an echo signal responsive to the second successive pulse.

58. The ultrasonic imaging system of claim 43 wherein each of the ultrasonic pulses transmitted into the body have a range of frequency components, the range of frequency components including the fundamental frequency component.

of frequency components including the fundamental frequency component.

59. A display device displaying a ^{and image processor together forming and} ~~3~~^{three} dimensional image of an interior of a ^{tissue or fluid} body, the ^{Three} ~~3~~-dimensional image being formed from harmonic frequency echo signals generated by interaction of fundamental frequency ultrasound signals with ultrasound reflectors within the body.

60. The display device^{and IP} of claim 59 wherein the 3-dimensional image is further formed from fundamental frequency echo signals generated by the reflections of the

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69. The display device of claim 59 wherein the 3-dimensional image is formed from harmonic frequency echo signals generated by interactions of fundamental frequency ultrasound signals solely with tissues within the body.

70. The display device of claim 59 wherein the fundamental frequency ultrasound signals have a range of frequency components, the range of frequency components including the fundamental frequency.

71 70. A method of generating a 3-dimensional image of ultrasound reflectors inside a body, comprising:

transmitting an ultrasound signal into the body, the ultrasound signal having at least a fundamental frequency;

detecting echoes of the transmitted ultrasound signal at a harmonic frequency that is a multiple of the fundamental frequency; and
using the detected echoes to form ^{the three-} a 3-dimensional image ^{of a tissue or fluid mass}

12. The method of claim 10, further comprising, prior to transmitting the ultrasound signal, introducing a contrast agent into the body.

13 72. The method of claim 70, further comprising:
detecting echoes of the transmitted ultrasound signal at the fundamental
frequency; and
using the detected echoes at both the fundamental frequency and the harmonic
frequency to form the 3-dimensional image.

74 73. The method of claim 72 wherein the detected echoes at the fundamental frequency are used to form the 3-dimensional image alternately with the use of the detected echoes at the harmonic frequency to form the 3-dimensional image.

⁷⁵ 74. The method of claim ⁷³ 72 wherein the detected echoes at the fundamental frequency and the detected echoes at the harmonic frequency are used simultaneously to form the 3-dimensional image.

⁷⁶ 75. The method of claim ⁷³ 72 wherein the detected echoes at the fundamental frequency are used to form portions of the 3-dimensional image that are at a greater depth within the body, and the detected echoes at the harmonic frequency are used to form portions of the 3-dimensional image that are at a shallower depth within the body.

⁷⁷ 76. The method of claim ⁷³ 72 wherein the detected echoes at the fundamental frequency are used to form portions of the 3-dimensional image that are at a greater depth within the body, the detected echoes at the harmonic frequency are used to form portions of the 3-dimensional image that are at a shallower depth within the body, and both the detected echoes at the fundamental frequency and the detected echoes at the harmonic frequency are used to form portions of the 3-dimensional image that are at an intermediate depth within the body.

⁷⁸ 77. The method of claim ⁷¹ 70 wherein the act of detecting echoes of the transmitted ultrasound signal comprises detecting echoes from moving ultrasound reflectors within the body.

⁷⁹ 78. The method of claim ⁷⁸ 77 wherein the act of using the detected echoes to form a 3-dimensional image comprise displaying the 3-dimensional image with indicia indicative of the velocity of the moving ultrasound reflectors.

⁸⁰ 79. The method of claim ⁷⁸ 77 wherein the act of using the detected echoes to form a 3-dimensional image comprise displaying the 3-dimensional image with indicia indicative of the intensity of the echoes reflected from the moving ultrasound reflectors.

⁸¹ 80. The method of claim ⁷¹ 70 wherein the act of transmitting an ultrasound signal into the body comprises transmitting an ultrasound signal into the body having a range of frequency components, the range of frequency components including the fundamental frequency.

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~~87.~~ The method of claim 81 wherein the act of transmitting ultrasonic signals into the body comprises transmitting ultrasonic signals having a range of frequency components, the range of frequency components including the fundamental frequency component.

89 88. A method of producing a ^{free} 3-dimensional ultrasonic image, comprising:

transmitting ultrasonic signals into the body, the transmitted ultrasonic signals having a fundamental frequency component;

receiving ultrasonic echoes from ^{the tissue or fluid} ultrasonic reflectors within the body, the received ultrasonic echoes containing both fundamental and harmonic frequency components;

detecting the fundamental and harmonic frequency components of the ultrasonic echoes;

forming signals that are a blend of the detected fundamental and harmonic frequency components;

storing the formed signals; and ^{of tissue or fluid}
displaying a ^{free} 3-dimensional image from the stored signals.

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90 89. The method of claim 88, wherein the blend of fundamental and harmonic frequency components varies as a function of time.

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91 90. The method of claim 88, wherein the blend of fundamental and harmonic frequency components varies as a function of the depth of the ultrasonic reflectors.

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92 91. The method of claim 88, wherein the blend of fundamental and harmonic frequency components varies as a function of the location of the ultrasonic reflectors

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93 92. The method of claim 88, further comprising, prior to transmitting the ultrasonic signals, introducing a contrast agent into the body.

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94 93. The method of claim 88, wherein the ultrasonic reflectors comprise a contrast agent.

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95 94. The method of claim 88 wherein the act of receiving echoes from ultrasonic reflectors within the body comprises receiving echoes from moving ultrasonic reflectors within the body.

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~~102 101.~~ The method of claim ~~88~~ wherein the detected fundamental frequency component is used to form portions of the 3-dimensional image that are at a greater depth within the body, the detected harmonic frequency component is used to form portions of the 3-dimensional image that are at a shallower depth within the body, and both the detected fundamental frequency component and the detected harmonic frequency component are used to form portions of the 3-dimensional image that are at an intermediate depth within the body.

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(d) forming the three-dimensional reconstruction in response to said information signals.

wherein the three-dimensional reconstruction is responsive to said information signals.

(a) transmitting ultrasonic energy at a first frequency band into a subject during said imaging session, said subject being free of added ultrasound contrast agent throughout the entire imaging session;

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¹⁰⁷~~106~~. A method for producing a three dimensional reconstruction with an ultrasound system, the method comprising the steps of: